

Overview: Beam Hardening Effect in X-ray CT

❖ Physical Acquisition Model:

- Attenuation coefficients are energy-dependent
- X-ray energy spectrum is broad.
- The measurement model is:

$$E[y_i | \mu] = -\log \left(\int_R S(E) \exp \left(-\sum_j A_{i,j} \mu_j(E) \right) dE \right)$$

- y_i is measurement, $\mu_j(E)$ is the attenuation coefficient
- A is the linear forward projection matrix
- $S(E)$ is the normalized energy spectrum

❖ Problem:

- Measurement is **non-linear function of attenuation coefficient**

❖ Possible Correction Approaches:

- Hardware pre-filtering,
- Dual energy CT,
- Linearization
- Model-Based Iterative Reconstruction (MBIR), etc.

Our Approach: Simultaneous IR and BHC in MBIR Framework

❖ A Simplified Poly-energetic X-ray Forward Model

Idea: Different materials can be separated according to their densities.

- Decompose energy-dependent attenuation into two unknown basis functions

$$\mu_j(E) = x_j \left((1-b_j)r_L(E) + b_j r_H(E) \right) \quad \leftarrow \text{Decouple location and energy}$$

- $b_j \in \{0, 1\}$ indicator of low or high material
- $r_L(E), r_H(E)$ two underlying basis energy-dependent functions

- Substitute the decomposition into the measurement model and obtain a polynomial parameterization using two **energy-independent "material" projections**

$$E[y_i | x] = h(p_{L,i}, p_{H,i}) = \sum_k \sum_l \gamma_{k,l} (p_{L,i})^k (p_{H,i})^l \quad p_{L,i} = \sum_j A_{i,j} x_j (1-b_j), \quad p_{H,i} = \sum_j A_{i,j} x_j b_j$$

Estimate others $\gamma_{k,l}$ online

- $p_{L,i}, p_{H,i}$ two energy-independent "material" projections
- $\gamma_{k,l}$ are the coefficients of the joint correction polynomial, can show $\gamma_{0,0} = 0, \gamma_{1,0} = \gamma_{0,1} = 1$

❖ MBIR-BHC (Simultaneous Image Reconstruction and Beam Hardening Correction)

$$\arg \min_{x \geq 0, \gamma} \left\{ \frac{1}{2} \sum_{i=1}^M w_i \left(y_i - \sum_k \sum_l \gamma_{k,l} (p_{L,i})^k (p_{H,i})^l \right)^2 + \text{regularization on } x \right\}$$

- Incorporate the poly-energetic X-ray forward model into MBIR objective function
- We **jointly estimate the coefficients** of the correction polynomial. **No additional spectrum information** is needed. Correction is adapted to the dataset being used.
- Material segmentation $b_j \in \{0, 1\}$ is calculated by thresholding the initial image fed into MBIR.
- Use **alternating optimization** over the image x and the polynomial coefficients $\gamma_{k,l}$

Experimental Results

❖ Simulated Data

- Simulated parallel-beam transmission polychromatic X-ray projections
- 720 views, 1 degree/view
- 1024 detectors, 0.24mm each
- 512x512 image, FOV = 250mm²
- Water disk phantom, with insertions of soft tissue and aluminum
- Severe streaks in FBP and generic MBIR
- Significant reduction in MBIR-BHC

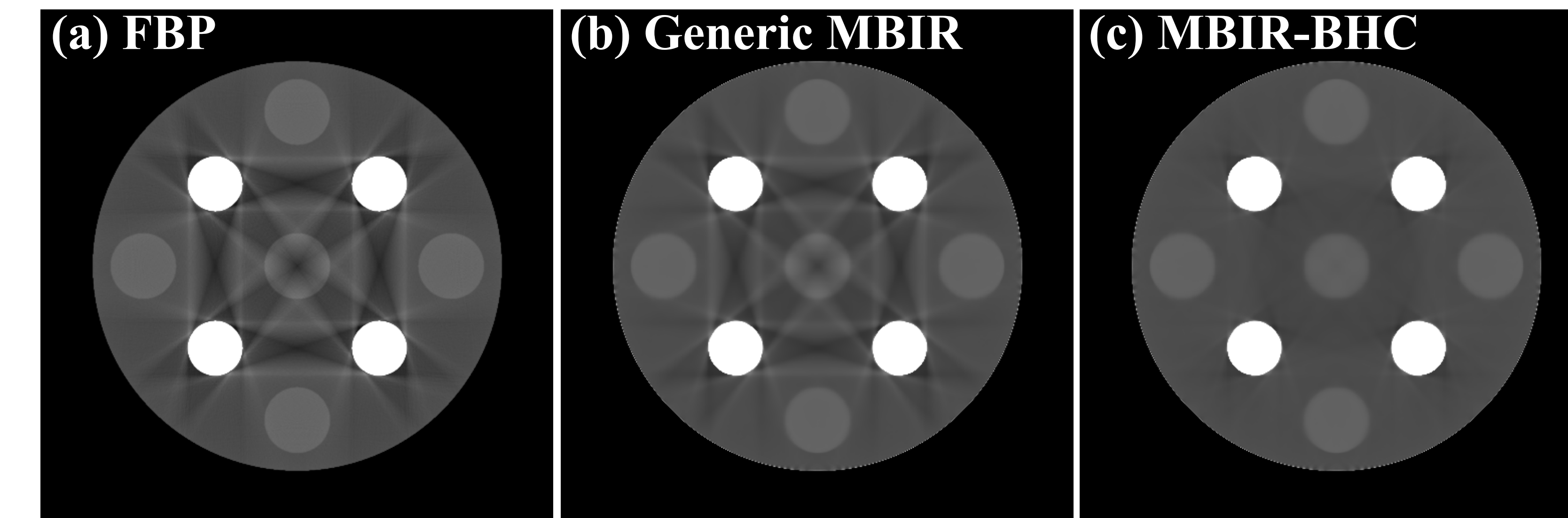


Fig. 1 Comparison of reconstructed image using the simulated dataset

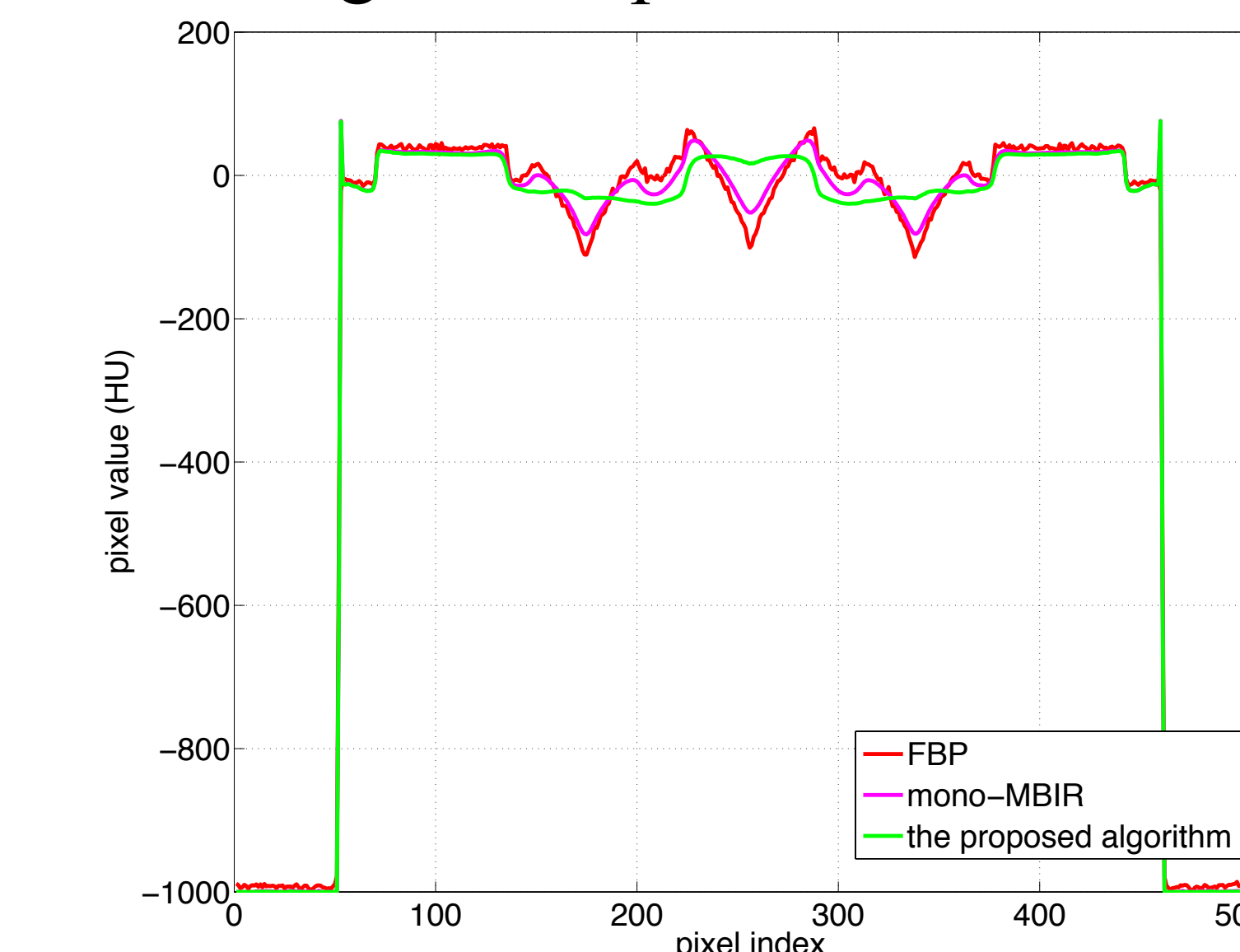


Fig. 2 Pixel profile of the simulation results

❖ Real X-ray CT Scan

- X-ray CT scan of an actual high clutter baggage with low and high density objects
- Resolution improvement
- Streak reduction
- Blooming artifacts reduction

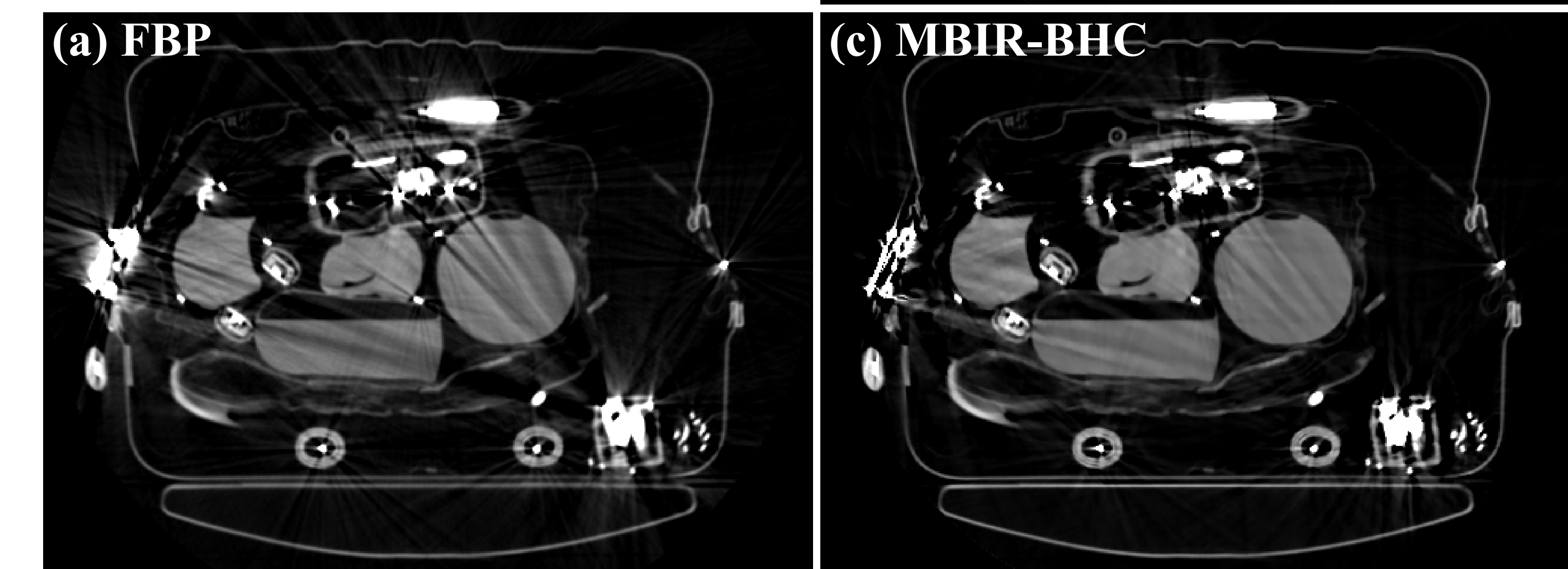


Fig. 3 Comparison of reconstructed image using the real X-ray CT data

Conclusions

- ❖ Incorporated a poly-energetic X-ray forward model using polynomial parameterization into MBIR
- ❖ Joint estimation of the image and coefficients of beam hardening correction function
- ❖ Simultaneous beam hardening correction during iterative reconstruction process
- ❖ No additional spectrum information needed, significant improvement in image quality

Acknowledgement

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