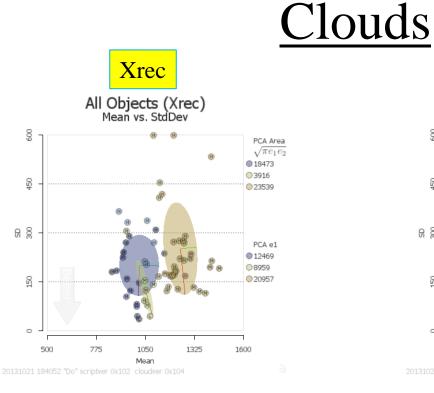
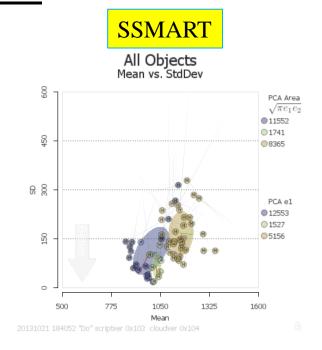


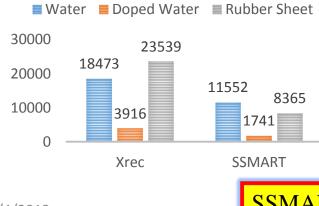
Sinogram-Sparsified Metal Artifact Reduction Technique (SSMART)

Massachusetts General Hospital And Harvard Medical School Synho Do, PhD

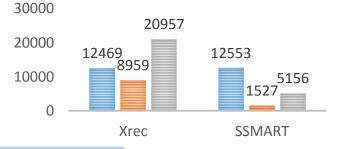




CLOUDS AREA



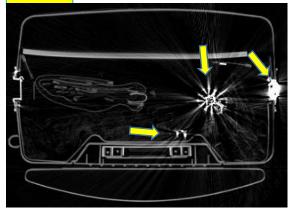


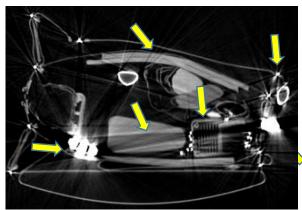


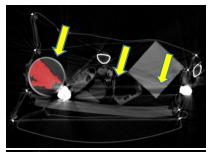
SSMART reduced cloud size.

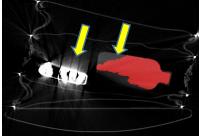
Image Comparison

Xrec

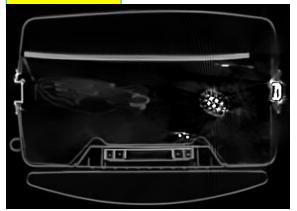






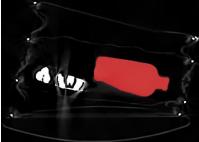


SSMART









- Less streaking and shading artifacts
- Better homogeneous regions reconstruction
- 194/2Better segmentation

Massachusetts General Hospital and Harvard Medical School



Synho Do, PhD Department of Imaging, MGH and Harvard Medical School 25 New Chardon Street, Suite 450 Boston, MA 02114 (email)



BIO NEWS PUBLICATIONS RESEARCH

Synho Do, PhD, is an <u>Assistant in Physics at Massachusetts General Hospital</u>, where he is a technical committee member of Webster Center for Advanced Research and Education in Radiation, and Instructor at Harvard Medical School. Dr. Do received the Ph.D. degree in Biomedical Engineering from University of Southern California. He is currently a member of IEEE Signal Processing Society, Bio–Imaging and Signal Processing (BISP). He is a MGH site PI for nVidia CUDA Research Center (CRC). Dr. Do's current research interests include statistical signal and image processing, estimation, detection, and medical signal and image processing, such as computed tomography. He has been a Co–Investigator for multiple medical imaging projects, and Co–PI/PI on medical (i.e., GE, Siemens, and Philips etc) and security (i.e., DHS, DARPA etc) image reconstruction projects.

http://scholar.harvard.edu/synho

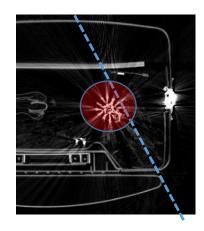
Nationality: U.S.A. (2013~present)

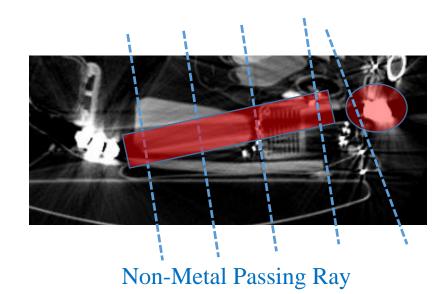
Latest News

DHS meeting

RSNA

Algorithm : Main Idea

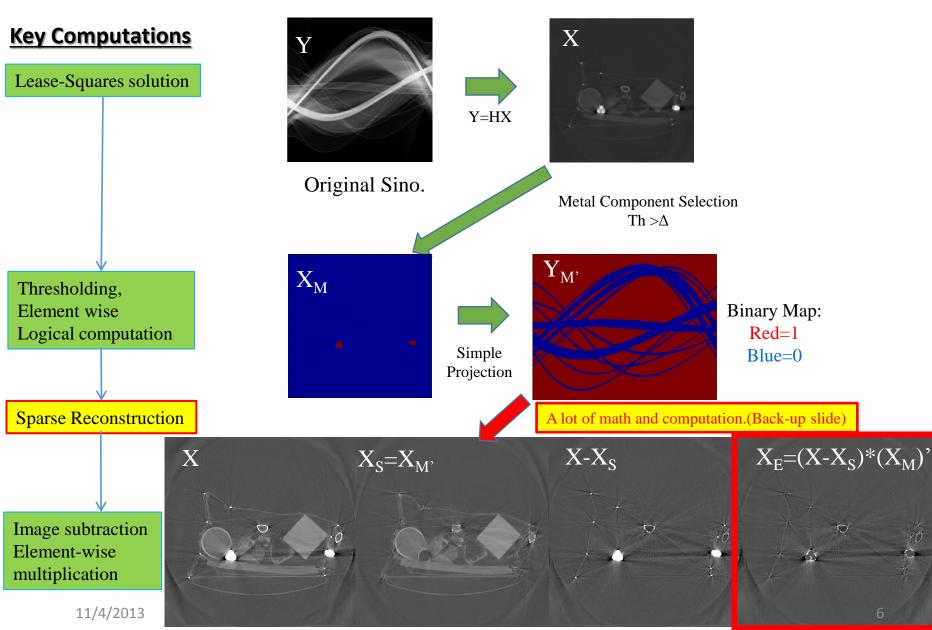




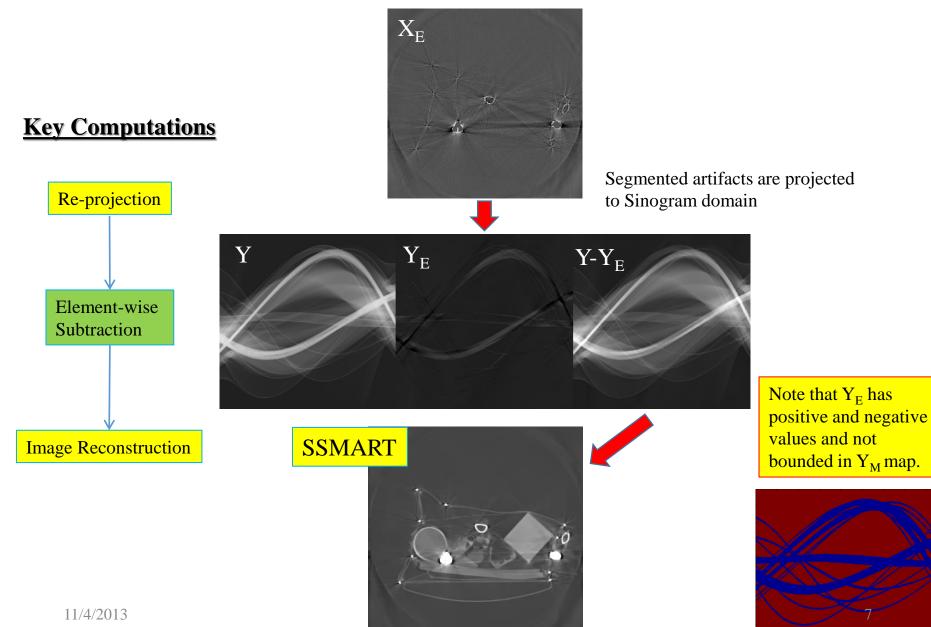
SSMART IDEA

- 1. <u>Don't use bad data</u>. → Throw it away
- 2. Let's use only non-metal passing rays for non-metal image reconstruction. (Use only Blue Ray-sums)
- 3. Let's <u>compensate</u> metal passing ray with segmentation and re-projection.

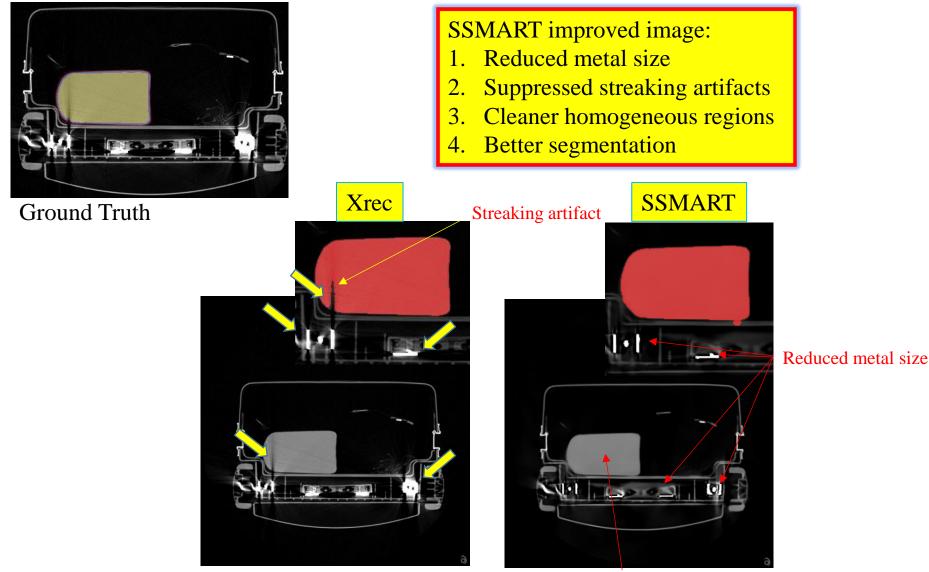
How SSMART works ? (1/2)



How SSMART works ? (2/2)



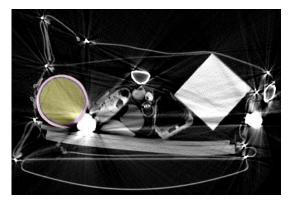
Streak artifacts reduction & segmentation (1/2)



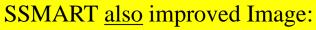
Streak artifacts reduction & segmentation (2/2)

Xrec

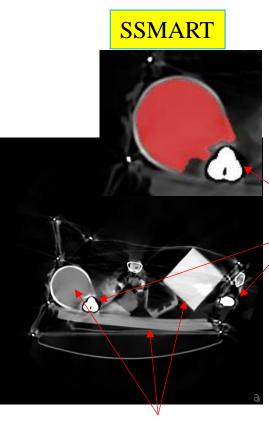
Shading artifact



Ground Truth



- 1. Shading artifacts
- 2. Big metal boundaries

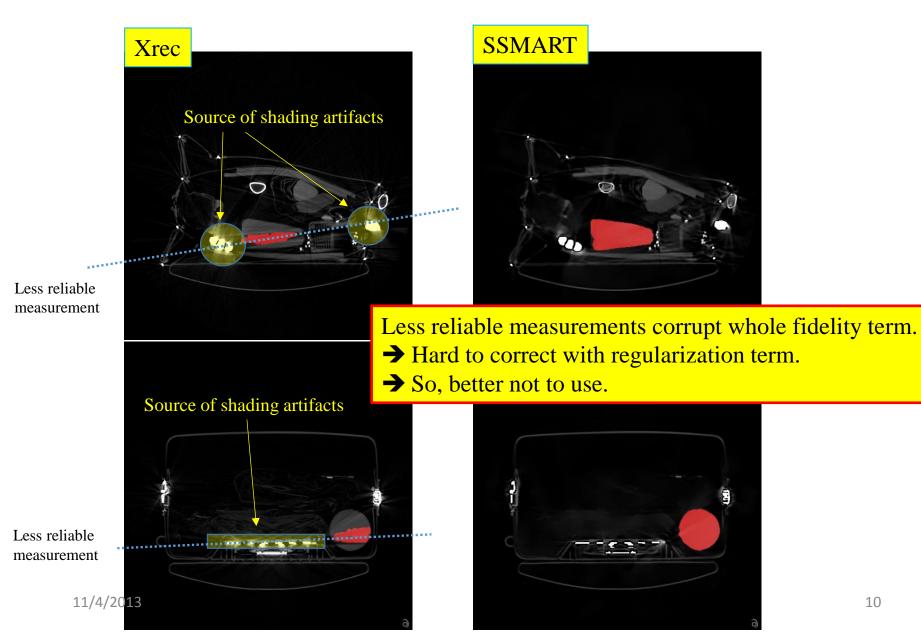


Cleaner metal boundaries

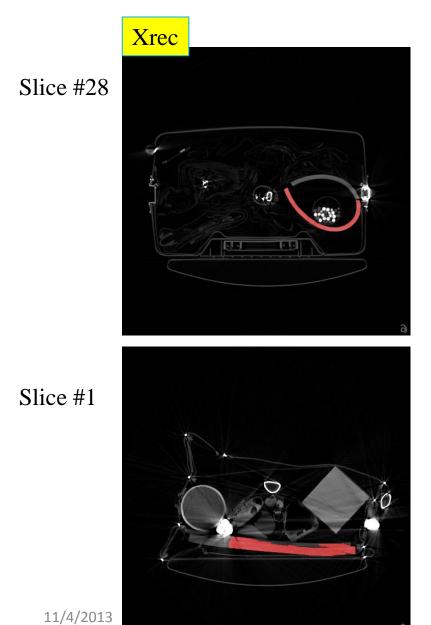
More uniform texture

11/4/2013

Shading Artifacts & Segmentation



Problem Cases



SSMART

No significant metal artifact but strong regularization



Removed shading artifact but no boundary recovery

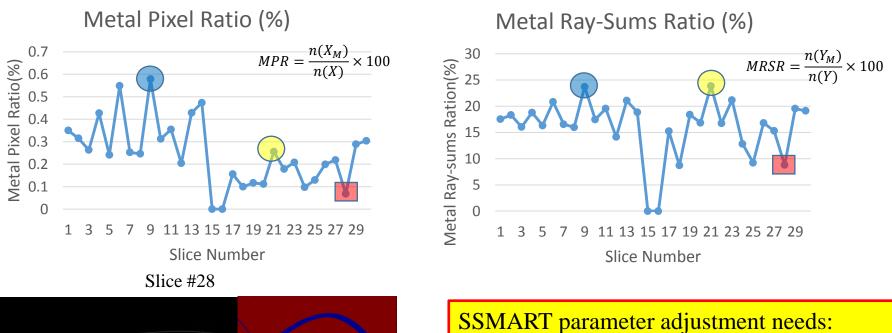


Parameter Selection Problem

Need Dual Energy ?

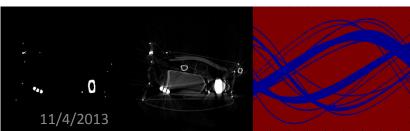
11

Sparseness vs. SSMART parameters



- 1. MPR and/or MRSR
- 2. Metal pixel intensity
- 3. Metal size







Xrec



Xrec





<u>Summary</u>

Strength

- Works well with small dense metal components.
- Great performance with a few objects.
- Removes low frequency shading artifacts.
- Improve homogeneity in uniform objects.

Weakness

- Not good for many metal components.
- Generates new streak artifacts when MPR & MRSR are high.
- Threshold sensitive.
- Additional projection required.

Future Research Topic

- More accurate system model would improve image quality. (Now, pencil-beam ray model and some artifacts near COR)
- Test with raw sinogram (less pre-processed) coupling with accurate system model. (Now, '.clp' is used)
- SSMART parameters can be adjusted by sparseness measurements.(Now, same parameters for all slices)
- Multi-level iterative threshold method can be tested. (Now, regardless pixel intensity and size of metal, all metal pixels are treated equally)

Back-up Slides

How SparseRecon works ?

- SparseRecon is <u>a modification of "image de-blurring</u>" [1,2]
- Iterative shrinkage algorithm

 $\hat{x} = \operatorname{argmin} \frac{1}{2} \|y - Ax\|^2 + \lambda \rho(x)$

x: image, y: sinogram, A: system matrix, λ : weighting parameter, and

 $\rho(x) = |x| - s \log(1 + \frac{|x|}{s})$

which leads to near *L1*-norm for small value of s>0 (s=0.0001 in our case).

- The new component : $A = H[\Psi, \Phi]$ Ψ and Φ are two *n x n* unitary matrices. And H is a conventional forward system matrix
- Therefore, the algorithm becomes to minimize:

$$\hat{x} = \operatorname{argmin} \frac{1}{2} \|y - H(\Psi x_{\Psi} + \Phi x_{\Phi})\|^2 + \lambda \rho(x_{\Psi}) + \lambda \rho(x_{\Phi})$$

^[1] M. A. Figueiredo, R. D. Nowak, and S. J. Wright, "Gradient projection for sparse reconstruction: Application to compressed sensing and other inverse problems," Selected Topics in Signal Processing, IEEE Journal of, vol. 1, pp. 586-597, 2007.

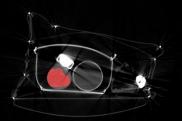
^[2] M. Elad, B. Matalon, and M. Zibulevsky, "Coordinate and subspace optimization methods for linear least squares with non-quadratic regularization," Applied and Computational Harmonic Analysis, vol. 23, pp. 346-367, 2007.

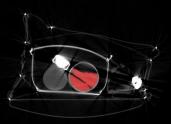
Xrec







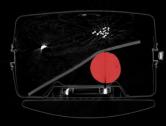


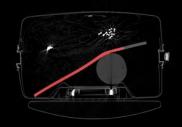


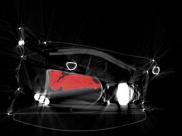


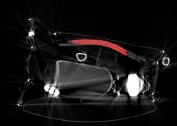






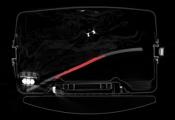


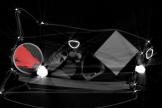












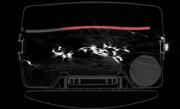


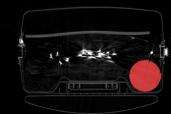


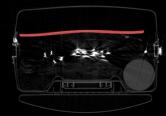








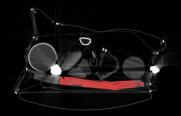








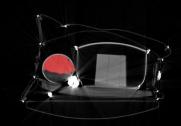












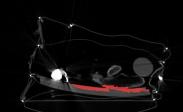


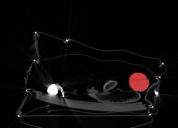


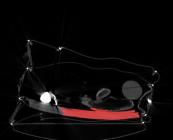


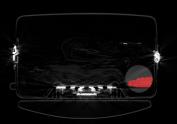








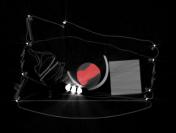


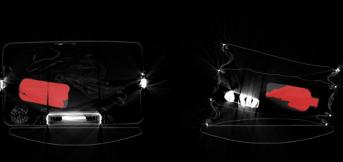




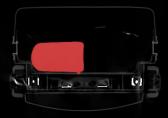












SSMART







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X. De







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